

# The Cyclodextrins as Modelling Agents of Drug Controlled Release

CATARINA M. FERNANDES and FRANCISCO J.B. VEIGA\*

Laboratory of Pharmaceutical Technology, Faculty of Pharmacy, University of Coimbra, 3000 Coimbra, Portugal

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# Abstract

The controlled release of nicardipine (NC) was achieved by hybridizing its hydrophilic and hydrophobic cyclodextrin (CDs) complexes, i.e., those with hydroxypropyl- $\beta$ -cyclodextrin (HP $\beta$ CD) and triacetyl- $\beta$ -cyclodextrin (TA $\beta$ CD), respectively. <sup>1</sup>H-nuclear magnetic resonance (<sup>1</sup>H-NMR) was performed to examine the interaction between both CDs and NC in solution. The solid complexes of NC : HP $\beta$ CD and NC : TA $\beta$ CD were prepared, in a 1 : 1 molar ratio by the spray-drying method. Complexation in the solid state was demonstrated by differential scanning calorimetry (DSC) and powder X-ray diffractometry. In vitro dissolution studies were carried out in simulated gastric (pH 1.2) and intestinal (pH 6.8) fluids, according to the USP basket method. The <sup>1</sup>H-NMR studies provided clear evidence of an interaction between the CDs and the aromatic rings of NC. The DSC thermograms of the solid complexes showed no endothermic peak due to NC melting and their diffraction pattern was completely diffuse, which suggested the formation of a novel type solid phase with an amorphous character. The low dissolution rate of NC, a weak basic drug, in alkaline medium was significantly improved by complexation with HP $\beta$ CD. In contrast, the *in vitro* release of this drug from the NC : TA $\beta$ CD complexes was markedly retarded in both dissolution media. An optimal formulation was then designed by the combination, in different molar ratios, of these two complexes. The release behavior of these preparations was investigated and it was observed that the retarding effect was dependent on the amount of the NC : TA $\beta$ CD complex. In addition, the initial release rate became faster as the molar ratio of the NC : HP $\beta$ CD complex increased.

# Introduction

Hydrophilic CDs derivatives such as methylated, hydroxyalkylated and branched CDs are useful to improve the low solubility, dissolution and bioavailability of poorly watersoluble drugs [1–3]. On the other hand, hydrophobic CDs like ethylated and peracylated derivatives have potential as slow/sustained-release carriers of drugs with short biological half-lives [4–6]. Thus, the critical combination of inclusion complexes obtained with these two kinds of CDs derivatives could be a promising drug delivery system, with a prolonged therapeutic effect.

In this study, NC was chosen as a model drug, since it is known that has a short-elimination half-life with significant fluctuations in plasma drug concentrations. NC bioavailability is very limited (15–40%), and like other dihydropyridine derivatives, its standard formulation undergoes rapid absorption and extensive biotransformation in the liver [7].

The interaction between NC and HP $\beta$ CD or TA $\beta$ CD was investigated in solution and in solid phase. In addition, the release behavior of these binary systems, as well the corresponding mixtures in different molar ratio, was evaluated in acidic (pH 1.2) and alkaline (pH 6.8) media.

## **Experimental**

## Materials

NC, HP $\beta$ CD (Kleptose HPB<sup>®</sup>, MW $\sim$ 1300, DS 0.63) and TA $\beta$ CD were purchased from Effechem SRL (Italy), Roquette (France) and Sigma-Aldrich (Germany), respectively.

# <sup>1</sup>H-NMR studies

The NC : HP $\beta$ CD and NC : TA $\beta$ CD samples were prepared in D<sub>2</sub>O and C<sub>2</sub>D<sub>5</sub>OD: D<sub>2</sub>O (50:50) mixture, respectively. The <sup>1</sup>H-NMR spectra of the pure components and their respective mixtures were obtained at 298 K on a Varian Unity-500 spectrometer using a 5-mm reverse detection NMR probe. The resonance at 4.8 ppm due to residual solvents (H<sub>2</sub>O and HDO) was used as internal reference. Chemical shits were calculated according to:  $\Delta \delta = \delta$ (complex)  $-\delta$  (free). The stoichiometry of the NC : CDs inclusion complexes was provided using the continuous variation technique (Job's plot) [8]. For each system, solutions with different CD or NC molar ratio were prepared, where the total molar concentration was kept constant, i.e., 5 mM and 2 mM for the NC: HP $\beta$ CD and NC: TA $\beta$ CD system, respectively. Samples were left overnight for equilibration before measurement.

A rotational Overhauser enhancement experiment (ROESY) for detection of intermolecular nuclear Over-

<sup>\*</sup> Author for correspondence. E-mail: fveiga@ci.uc.pt

hauser effects (NOEs) between NC and both CDs, was acquired for the 1:1 molar ratio at 298 K using the same probe. The ROESY experiments were performed with a mixing time of 500 ms and 100 ms for the NC: HP $\beta$ CD and NC: TA $\beta$ CD system, respectively.

## Preparation of solid complexes

The NC : HP $\beta$ CD complex was prepared by spray-drying as previously reported [9]. The NC : TA $\beta$ CD complex was also prepared by the spray-drying technique. Equimolar quantities of NC and CDs were dissolved in ethanol : water (50: 50). The resulting mixture was stirred for 24 h at room temperature and the obtained solution was subsequently spray-dried (LabPlant SD-05), under the following conditions: air flow rate – 50 m<sup>3</sup>/h; atomising air pressure – 1.0 Bar; inlet temperature – 160 °C, outlet temperature – 85 °C; flow rate of the solution – 400 ml/h. The product was sieved through a 63–160  $\mu$ m mesh.

Physical mixtures, in 1:1 molar ratio, of plain NC and CDs, were also prepared for reference.

## Characterization of the solid complexes

#### DSC studies

DSC measurements were performed on a Shimadzu DSC-50 differential scanning calorimeter. All samples accurately weighed (1 mg of NC or its equivalent) were placed in sealed aluminium pans, before being heated under nitrogen flow (20 ml/min) at a scanning rate of 10 °Cmin<sup>-1</sup>, from 25 °C to 200 °C (for the NC : HP $\beta$ CD system) or to 230 °C (for the NC : TA $\beta$ CD system).

## X-ray diffractometry

The powder X-ray diffraction patterns were recorded using a Philips X'Pert, model PW3040/00 diffractometer, with Co as anode material and a graphite monochromator, operated at a voltage of 40 Kv and a current of 35 mA. The samples were analyzed in the  $2\theta$  angle range of 5–50° and the process parameters were set as: scan step size of 0.025° ( $2\theta$ ), scan step time of 1.25 s and time of acquisition of 1 h.

## Dissolution studies

The dissolution profiles were collected using a Vankel VK7000 apparatus, according to the USP rotating basket method. The dissolution media consisted of 1000 ml of enzyme-free simulated gastric (pH 1.2) and intestinal (pH 6.8) fluids (USPXXIV). Powdered samples (n = 6) containing 30 mg of NC or its equivalent were used. The stirring speed was 100  $\pm$  2 rpm and the temperature was maintained at 37  $\pm$  0.2 °C. At settled time intervals up to 8 hours, the concentration of dissolved drug was automatically determined by UV spectroscopy at 357 nm.

## **Results and discussion**

## <sup>1</sup>H-NMR studies

The drug: CDs interaction in solution was based on the modification of the <sup>1</sup>H-RMN spectrum of NC upon complexation. The <sup>1</sup>H-NMR spectra reporting the protons of TA $\beta$ CD, NC, and NC : TA $\beta$ CD mixture (1 : 1) are presented in Figure 1. Among the different detected signals, those corresponding to the F, O, N and M protons and also the G proton of NC were the most affected ( $\Delta \delta = 0.016$  ppm) by the presence of TA $\beta$ CD. Similarly, in the NC : HP $\beta$ CD system (not shown) the F, O, N and M protons and the G proton of NC experienced a pronounced shift variation, i.e.,  $\Delta \delta = 0.020$  and 0.025 ppm, respectively.

The stoichiometry for both complexes was established by application of the continuous variation method, which followed the changes in chemical shifts of the G proton, for the NC : HP $\beta$ CD system, and of the F, O, N and M protons for the NC : TA $\beta$ CD system (Figure 2). Both plots demonstrated a 1 : 1 stoichiometry, since the maximum was at  $r_{NC} = 0.5$ .

From these results, we could propose the coexistence in solution of two different complexes with 1 : 1 stoichiometry, concerning the nitro-phenyl ring and the other phenyl group of the drug. Similar results have been obtained by other authors [10]. This assumption was further confirmed by ROESY experiments (not shown). The ROESY spectra of complexes showed the existence of intermolecular NOEs between several phenyl ring protons (F, O, N, M and G) of NC and the HP $\beta$ CD protons and also between the drug F, O, N and M protons and the TABCD protons, specially those from the acetyl groups.

#### Characterization of the solid complexes

The complete disappearance of the NC endothermic peak at ca. 174 °C was observed in the NC : HP $\beta$ CD spraydried system (Figure 3). Similarly, the NC : TA $\beta$ CD complex showed no endothermic peaks, due to the melting of both components (Figure 4). These results suggest the formation of an amorphous solid dispersion, the molecular encapsulation of the drug inside the CD cavity, or both [11].

As shown in Figure 5, the diffractograms of the physical mixtures were constituted practically by the simple superposition of each single component, indicating the presence of NC in the crystalline state. In opposite, the spray-dried systems displayed somewhat diffuse diffraction patterns, indicating the amorphous nature of NC. The presence of a new solid phase with lower crystallinity than the drug may be attributed to an interaction between NC and both CDs, where a possible complexation of NC inside the CDs cavity was contemplated [12], corroborating the DSC observations.

#### Dissolution studies

The dissolutions profiles of NC and NC: CDs binary systems in simulated gastric (pH1.2) and intestinal (pH 6.8) fluids are presented in Figures 6 and 7, respectively. The dissolution characteristics of NC, a weak basic drug, were



Figure 1. <sup>1</sup>H-NMR spectra of TA $\beta$ CD (A), NC (B) and NC : TA $\beta$ CD (1 : 1) mixture (C).



*Figure 2.* Job's plots corresponding to the chemical shift displacement of the F, O, N, M ( $\bullet$ ) and the G ( $\blacktriangle$ ) protons of drug for the NC : TA $\beta$ CD and NC : HP $\beta$ CD system, respectively.



Figure 3. DSC thermograms of NC (A), HP $\beta$ CD (B), NC : HP $\beta$ CD physical mixture (C) and NC : HP $\beta$ CD (D) spray-dried system.



Figure 4. DSC thermograms of NC (A), TA BCD (B), NC : TA CD physical mixture (C) and NC : TA CD (D) spray-dried system.



*Figure 5.* X-ray diffractograms of NC (A), HP $\beta$ CD (B), NC: HP $\beta$ CD physical mixture (C) and NC: HP $\beta$ CD spray-dried system (D), TA $\beta$ CD (E), NC: TA $\beta$ CD physical mixture (F) and NC: TA $\beta$ CD spray-dried system (G).



Figure 6. Dissolution profiles of NC and NC : HP $\beta$ CD and NC : TA $\beta$ CD systems at pH 1.2.



*Figure 7.* Dissolution profiles of NC and NC : HP $\beta$ CD and NC : TA $\beta$ CD systems at pH 6.8.



*Figure 8.* Dissolution profiles of (NC : HP $\beta$ CD complex): (NC : TA $\beta$ CD complex) in different molar ratios at pH 1.2.



Figure 9. Dissolution profiles of (NC : HP $\beta$ CD complex): (NC : TA $\beta$ CD complex) in different molar ratios at pH 6.8.

significantly improved by complexation with HP $\beta$ CD, specially in alkaline medium. In contrast, the drug release rate from the NC : TA $\beta$ CD spray-dried complex was markedly retarded in both media.

An optimisation of the release profile of NC was further attempted by changing the mixing ratio of each complex in the formulation. The release profiles of NC from formulations consisting of mixtures of NC : HP $\beta$ CD and NC : TA $\beta$ CD complexes in various molar ratios, at pH 1.2 and pH 6.8 are presented in Figures 8 and 9, respectively.

The drug release from the different formulations occurred in two stages: faster release in the initial stage (up to 1 hour) and slower release in the second stage. It is evident that TA $\beta$ CD retarded the drug release rate, being this retarding effect dependent on the amount of hydrophobic complex in the formulation. On the other hand, the initial release rate of the drug increased with increasing amount of the hydrophilic complex. Among the various combinations, we selected the 1 : 4 formulation to further in vivo studies in rabbits.

From the above reported data it was mainly concluded that the drug release could be arbitrarily controlled by the combination of hydrophilic and hydrophobic complexes in an appropriate molar ratio.

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