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13 We explore the concept of modulating neural stem cells and their 14 15 niches for brain repair using nanotechnology-based 16 approaches. 17 These approaches include stimulating cell proliferation, recruitment, 18 19 and differentiation to functionally 20 recover damaged areas. Nanoscale-engineered materials poten-21 tially overcome limited crossing of 22 the blood-brain barrier, deficient 23 24 drug delivery, and cell targeting.

25 From Neural Stem Cells to 26 Nanomedicine

27 No therapies are yet available to fully 28 restore loss of brain function. One of the 29 therapies explored in several preclinical 30 trials is the transplantation of neural stem 31 cells (NSCs) or their progenies [1]. How-32 ever, cell survival is poor, and the integra-33 tion of transplanted cells into the neural circuitry is uncertain. An alternative is to 34 35 manipulate endogenous NSCs (Box 1). In 36 this case, the patient would benefit from his 37 own cells, bypassing the use of invasive 38 and costly transplantation procedures. 39 Nanoparticulate systems for brain delivery 40 (e.g., anticancer drugs, analgesics, anti-41 Alzheimer's and anti-Parkinson's drugs) 42 have been described in the past 25 years 43 [2]. However, modulation of the activity/ 44 differentiation of NSCs by nanoparticulate 45 systems releasing small molecules was

only recently demonstrated [3,4]. Current progress in the nanomedicine field has been stimulated by better understanding the biology of NSCs and by identifying molecular players capable of modulating their activity, proliferation, migration, and differentiation. This new avenue of research requires the development of advanced nanomaterials that, in some cases, have the capacity to transport drugs across the blood-brain barrier (BBB), target NSCs, deliver their payloads at the cell cytoplasm, and efficiently activate membrane receptors. Ideally, these materials should combine multiple features such as targeting, traceability, high cellular internalization and endolysosomal escape, release of multiple biomolecules at different timepoints and dosages, and biodegradation.

Modulation of Endogenous NSCs

Brain delivery of nanostructured materials can be performed by intracerebroventricular/intracerebral infusion or disruption of the BBB (e.g., by ultrasound). These approaches maximize the amount of drug that reaches the target site. Alternatively, systemic delivery by intravenous (i.v.) or intraperitoneal (i.p.) injections circumvents the need for invasive stereotaxic surgery. To maximize the BBB permeation, nanostructured materials, such as nanoparticles (NPs), can be coated with ligands or antibodies recognized by receptors/transporters or epitopes on brain endothelial cells. Few reports explore the biodistribution of NPs injected intravenously in distinct brain regions (that can be specifically affected by neurodegenerative diseases) and the ability of NPs to escape from vasculature into the brain parenchyma. Additionally, nanomaterials can incorporate peptide ligands to specifically target endogenous NSCs. Some ligands have been identified by phage display peptide libraries [5]. Importantly, functionalized nanostructured hydrogels were shown to successfully induce NSC differentiation while supporting tissue regeneration [6]. Recently, we have successfully developed a NP formulation capable of controlling NSC differentiation both in vitro and in vivo [3,4]. Contrary to soluble

retinoic acid (RA), our results demonstrated that RA-NPs injected intracerebroventricularly contributed to the successful neuronal commitment of mouse subventricular zone (SVZ) NSCs.

Nanomedicine Approaches for Stroke

Stroke is the consequence of blood supply disruption to the brain. In the human brain, stroke stimulates neurogenesis and neuroblast migration to the site of injury. However, the number of neurons generated by NSCs in the postischemic brain is insufficient (approximately 0.2% of the cells lost), and their survival is minimal. Therefore, enhancing NSC activity provides a promising therapeutic platform for stroke. For example, polymeric NPs containing epidermal growth factor (EGF, which stimulates NSC proliferation) or erythropoietin (EPO, which reduces apoptosis of NSC-derived differentiated cells) have been encapsulated in a hyaluronan methylcellulose hydrogel and implanted in the epicortical region of the brain (2-3 mm from the SVZ region). In these conditions, EGF was completely released within the first week, while EPO was released for 3 weeks. The role of NP was to control the release of bioactive agents within the gel without any targeting role to the stem cell population. The sequential release of both molecules regenerated the peri-infarct region, which was correlated with an increase in SVZ NSC proliferation [7]. This biomaterial approach may be an alternative to intracerebroventricular infusion by a catheter/minipump system, as demonstrated in preclinical tests. Additionally, self-assembling peptide nanofiber scaffolds tested in a rat model of hemorrhagic stroke reduced brain injury and supported the secretion of neuroprotective trophic factors while being disassembled [8]. It would also be interesting to further explore this outcome on the neurogenic niches.

Nanomedicine Approaches for Parkinson's Disease

Parkinson's disease (PD) is a disorder characterized by the degeneration of 93

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Box 1. Neural Stem Cell Biology

The discovery that neural stem cells (NSCs) are present in the adult mammalian brain throughout life raised many expectations among the medical and scientific community. NSCs have the ability to produce new neurons, astrocytes, and oligodendrocytes and are located in two main neurogenic niches: the subventricular zone (SVZ) lining the walls of the lateral ventricles and the subgranular zone (SGZ) of the hippocampus. These niches are formed by NSCs and surrounding support cells, such as progenitor cells, neurons, astrocytes, endothelial cells, and microglia. In physiological conditions, new neurons derived from the SVZ, the largest NSC pool, migrate towards the olfactory bulb in rodents, originating interneurons, or towards the striatum in humans, originating striatal neurons. Neurogenesis also persists throughout life in the hippocampal SGZ, however, with a smaller pool of NSCs. In response to injury, NSCs proliferate and migrate to the lesioned site, and differentiate into new neurons. Owing to these unique characteristics, targeting NSCs rather than somatic neural cells might be beneficial from a regenerative perspective since NSCs are considered to be an inexhaustible source of new neurons are able to survive under the injured environment. For that reason, nanoparticulate systems are a promising tool to modulate NSC activity, self-renewal, survival, proliferation, migration, differentiation, and functional integration into neural circuits in the context of neurodegeneration.

96 dopaminergic neurons in the substantia 97 nigra pars compacta, which leads to the 98 depletion of dopaminergic fibers in the 99 striatum and consequently originates 100 motor symptoms. Several contradictory 101 reports showed that neurogenesis is 102 altered in PD. By modulating NSCs, new 103 dopaminergic neurons could repopulate 104 the lesioned striatum. The combination 105 of hepatocyte growth factor (HGF)-loaded hydrogels with leukemia inhibitory factor 106 107 (LIF)-loaded NPs significantly mobilized 108 human NSCs in vitro [9]. Both molecules 109 induced NSC migration according to their 110 release profile: HGF and LIF induced 111 migration for approximately 2 and 112 5 weeks, respectively. A separate study 113 has shown that a multifunctional bio-114 material comprising an injectable multi-115 functional gelatin-hydroxyphenylpropionic 116 acid hydrogel and dextran sulfate/chitosan 117 polyelectrolyte complex NP loaded with 118 stromal cell-derived factor $1 \propto (SDF-1 \propto)$ 119 is a very promising therapy for cavity brain 120 lesions by recruiting endogenous NSCs 121 and enhancing neural tissue regeneration 122 [10]. The role of the NPs was to provide 123 the desired release kinetics of SDF-1 \propto to 124 recruit NSCs and progenitor cells, while 125 the gel was to provide a compatible 126 structural support for cell homing before 127 matrix remodeling. Therefore, the combi-128 nation of nanomedicine with tissue engi-129 neering may be suitable for PD brain 130 repair. Further preclinical studies are needed to show the relevance of this 131 132 approach.

Nanomedicine Approaches for Alzheimer's Disease

Alzheimer's disease (AD) is the most prevalent type of dementia characterized by synaptic and neuronal loss in brain areas such as the entorhinal cortex, hippocampus, and neocortex, which are essential for memory and other mental abilities. The transplantation of NSCs, genetically altered or stimulated with proneurogenic factors, were able to rescue spatial and memory deficits in several AD animal models [11,12]. However, cell replacement can also be achieved by modulating the endogenous neurogenic 133 niche of the hippocampus. Recently, it 134 was demonstrated that poly(lactic-co-gly-135 colic acid) (PLGA) NPs containing curcu-136 min are capable of inducing neurogenesis 137 and reverse learning and memory impair-138 ments in a rat model of AD [13]. The role of 139 NPs was to increase the bioactive agent 140 neuroprotective efficacy, reduce the 141 required dose, and facilitate the transport 142 through the BBB without compromising 143 its integrity. Moreover, polymeric conju-144 gates (100 nm) based on hyaluronic acid 145 conjugated with multiple molecules of 146 ephrin-B2 and sonic hedgehog per poly-147 mer chain have also been successfully 148 used to stimulate neurogenesis in normally 149 quiescent regions of the brain [14]. The 150 multivalent ligand induced a sixfold 151 increase in the fraction of newly divided 152 neuronal precursors in the adult rat 153 striatum. 154

Future Outlook

The modulation of NSC activity by nanomedicine approaches would represent a significant step towards the development of new brain repair therapies. However, several issues remain to be solved. An 155

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Figure 1. Modulation of Neural Stem Cells (INSCs) Either at the Neurogenic Niche or at Non-Neurogenic Regions, such as the Striatum or Cortex. In the neurogenic niche (A), nanoparticles (NPs) can specifically target receptors expressed by NSCs (I). Alternatively, NPs may target other cellular components of the stem cell niche, which in turn secrete factors that modulate the activity/differentiation of NSCs (II). In a nonneurogenic region (B), NPs may initially release factors to recruit NSCs (I) and subsequently to differentiate them (II), acting extra- or intracellularly.

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161 important subject is to identify NSC epit-162 opes to specifically target this cell population in vivo (Figure 1A). This effort will 163 increase both the specificity and the effi-164 165 ciency of nanomedicine platforms while 166 reducing potential side effects. Another 167 important concern is to better understand 168 the NSC niche upon injury. It is possible 169 that the manipulation of actively proliferat-170 ing progenitor cells rather than quiescent 171 cells would be more efficient. Importantly, 172 an understanding of the pathology pro-173 cesses and signaling pathways involved 174 are critical elements to consider when 175 selecting an appropriate nanomaterial for 176 brain therapy.

177 Although the great majority of published studies acted on neurogenic regions, 178 179 nanostructured materials might also boost 180 neurogenesis in non-neurogenic regions 181 (e.g., striatum, cortex). In this case, bio-182 materials should first recruit NSC or pro-183 genitor cells and then induce their 184 differentiation by the delivery of neurogenic factors (Figure 1B). Accomplishing 185 this goal requires the development of 186 187 materials able to release multiple bioactive 188 molecules at different times and dosages.

Acknowledgments

This work was funded by Fundação para a Ciência e Tecnologia (FCT), FEDER, and COMPETE (PTDC/SAU-NEU/104415/2008, FCOMP-01-0124-FEDER-041099, SFRH/BD/79526/2011), L'Oréal-UNESCO Portugal for Women in Science, EC (ERC project no. 307384, 'Nanotrigger'), COMPETE (Centro-07-ST24-FEDER-002008), FEDER funds through POCI-COM-PETE2020 Operational Programme Competitiveness and Internationalization in Axis-I (POCI-01-0145-FEDER-007491), and by FCT (UID/Multi/00709/2013).

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http://dx.doi.org/10.1016/j.tibtech.2016.02.003

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